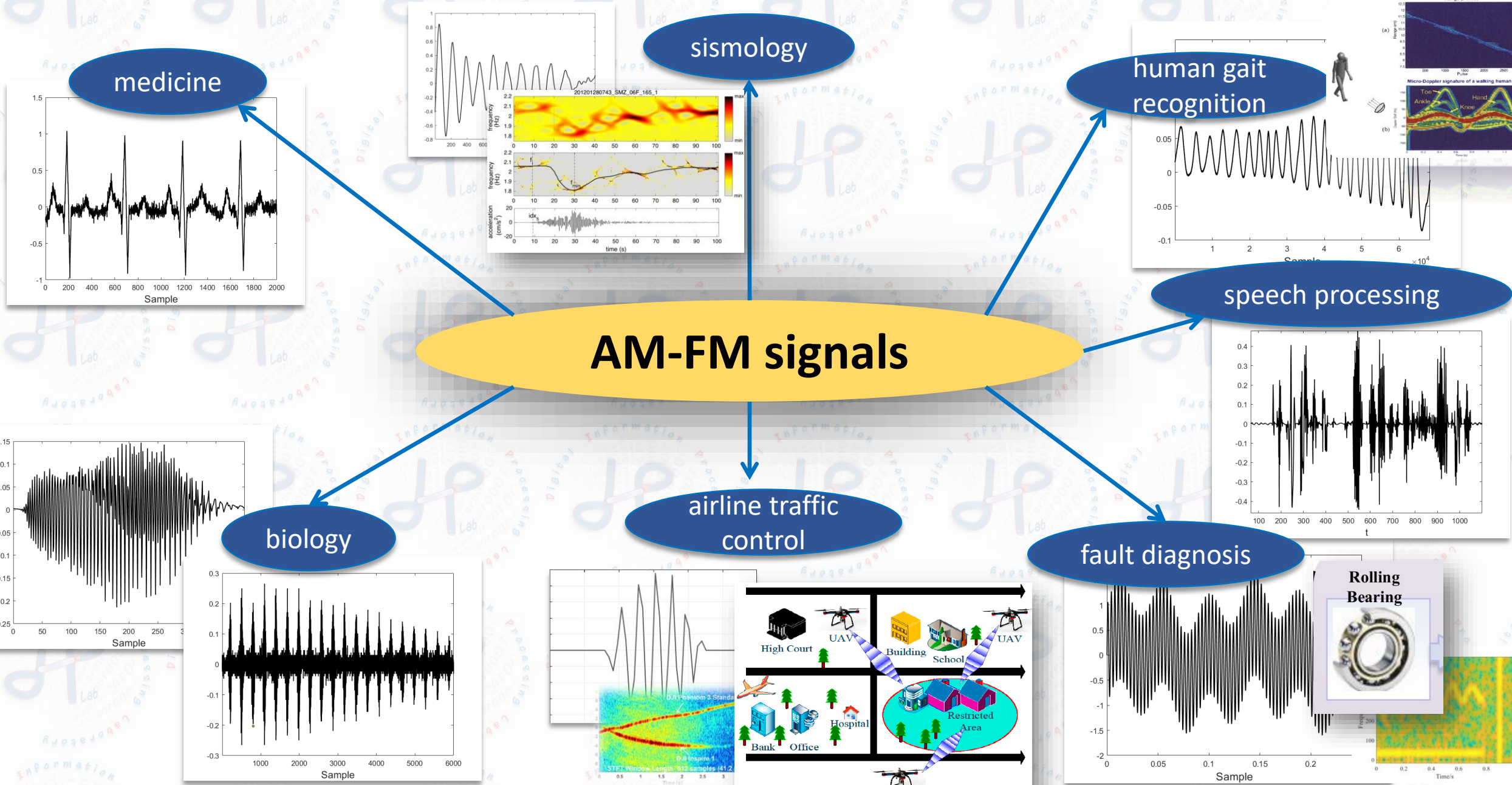


Signal modes counting@DIPLab

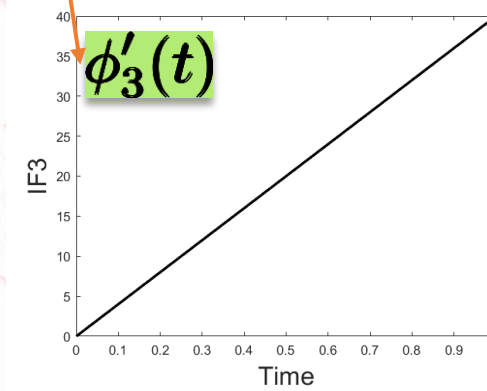
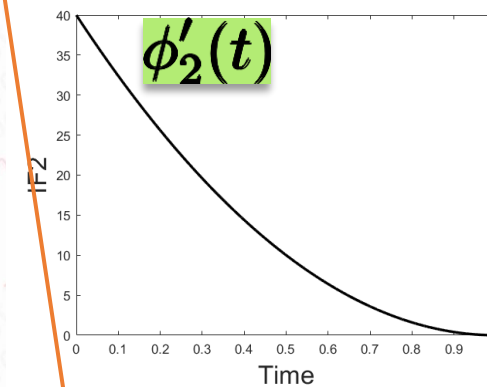
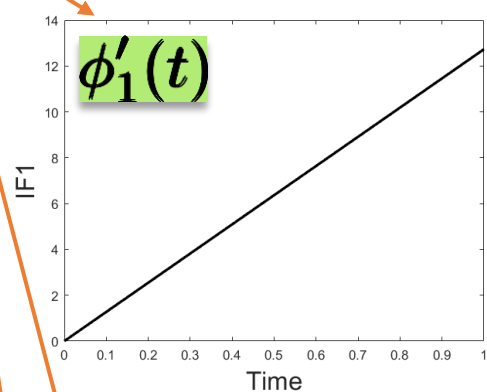
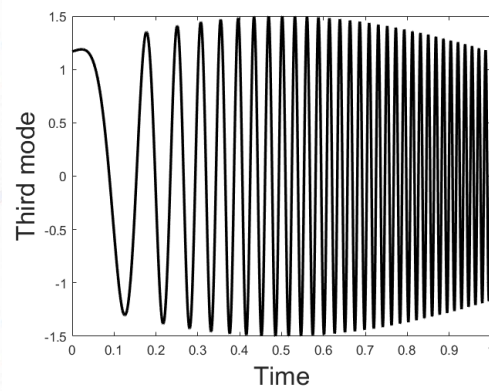
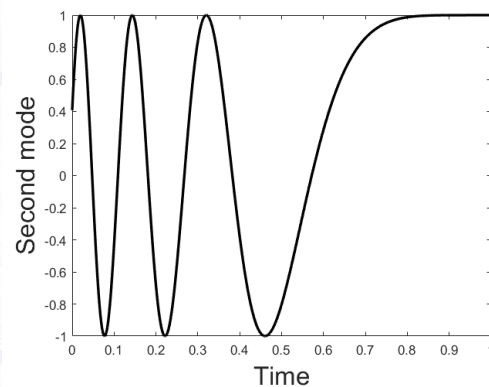
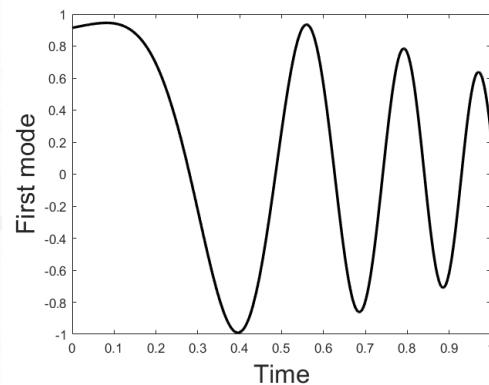
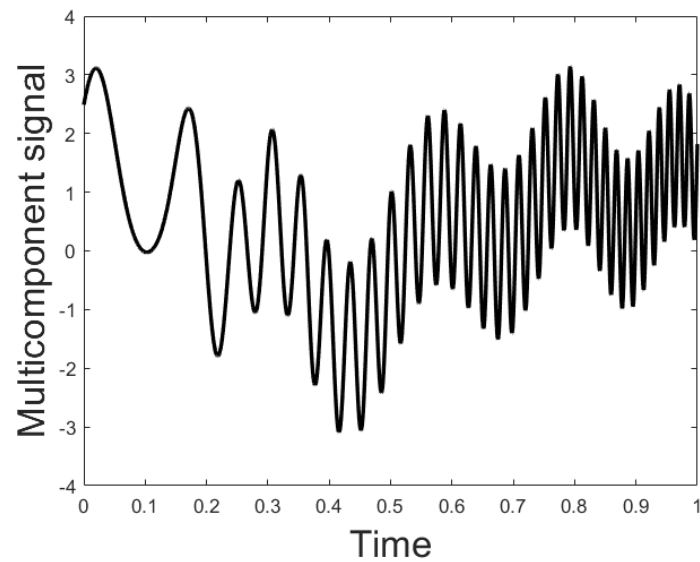


Amplitude and Frequency Modulated signals everywhere



Instantaneous Frequency (IF)

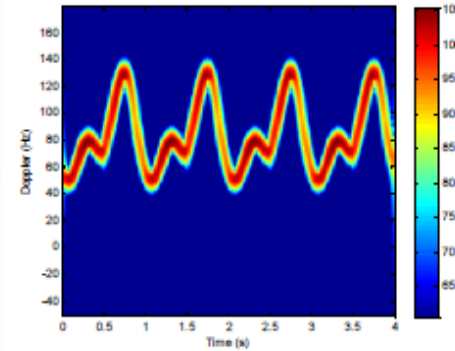
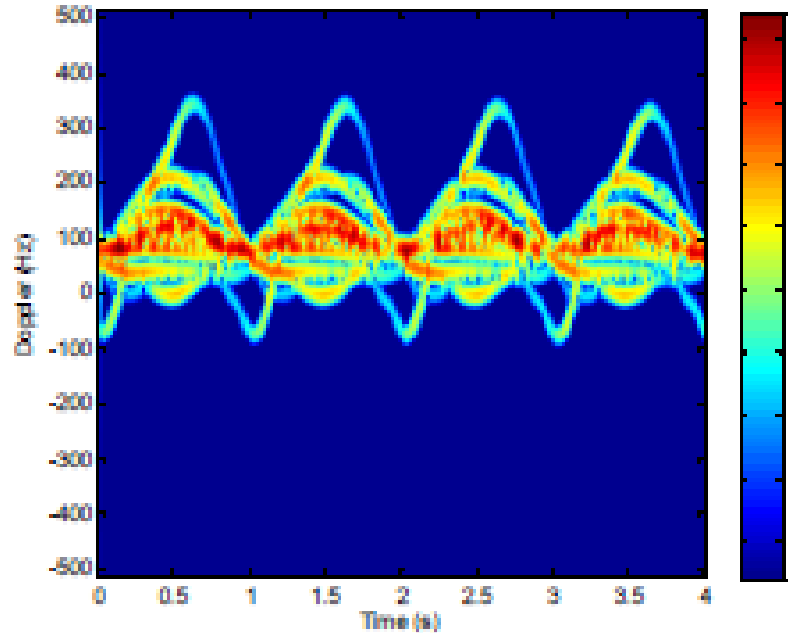
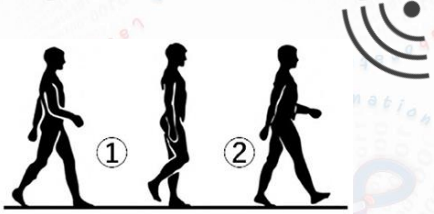
$$f(t) = \sum_{k=1}^N f_k(t) = \sum_{k=1}^N a_k(t) e^{i\phi_k(t)}$$



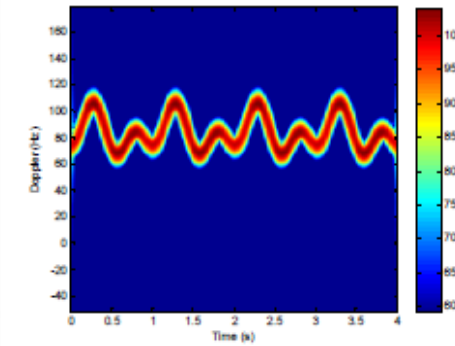
Instantaneous Frequency (IF): human gait recognition

Microdoppler signature of human body: walk

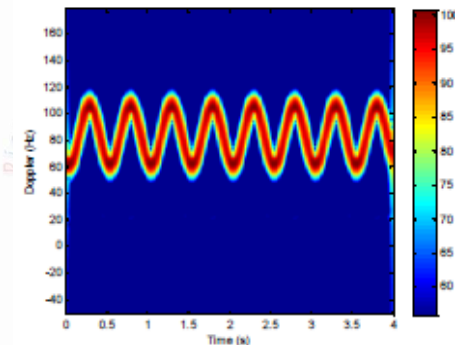
IF = speed of human body components



$\phi'_1(t)$ Leg



$\phi'_2(t)$ Arm



$\phi'_3(t)$ Head

Main contribution

Definition of local and pointwise methods for TF analysis of frequency modulated multicomponent signals having non separable modes

spectrogram evolution law and weakened separability

method

- iterative reassignment
- skeleton-based reassignment
- pde-based IF curves reconstruction
- Radon transform based IF estimation

advantages

- ✓ non parametric approaches
- ✓ independency of IF functional class
- ✓ better modes reconstruction in TF interference (non separable) region
- ✓ robustness to moderate noise

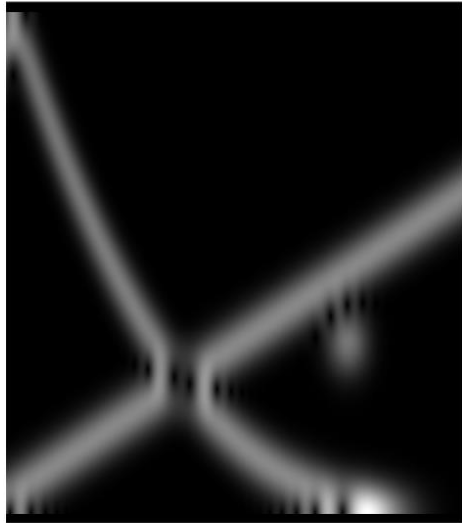
requirements

modes counting and interference region detection

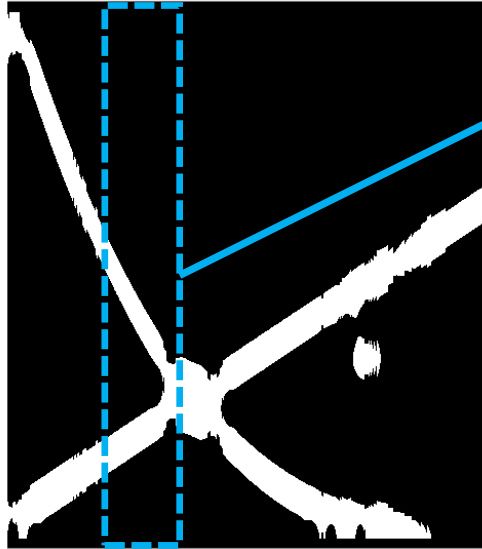
Modes counting

$$\frac{\partial P(u, \xi)}{\partial u} + \phi''(u) \frac{\partial P(u, \xi)}{\partial \xi} - \frac{2a'(u)}{a(u)} P(u, \xi) = 0$$

Spectrogram



Binarization
and Run Length
Encoding (RLE)



best threshold
by Minimum Description
Length

$N_{\text{modes}} = 2$

$N_{\text{modes}} = 2$

...

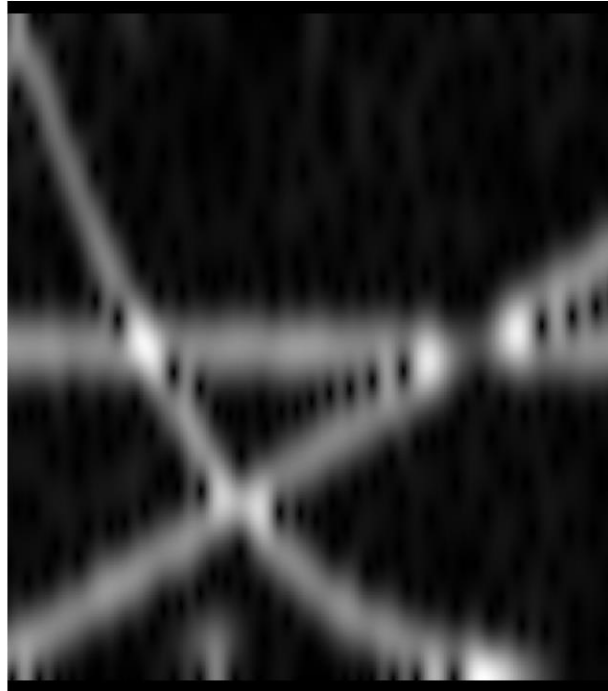
sequential columns

Modes
OVERLAPPING is
detected so that
the
CORRECT NUMBER
of modes is
estimated, for each
time instant

$N_{\text{modes}} = 2$

Modes counting: results

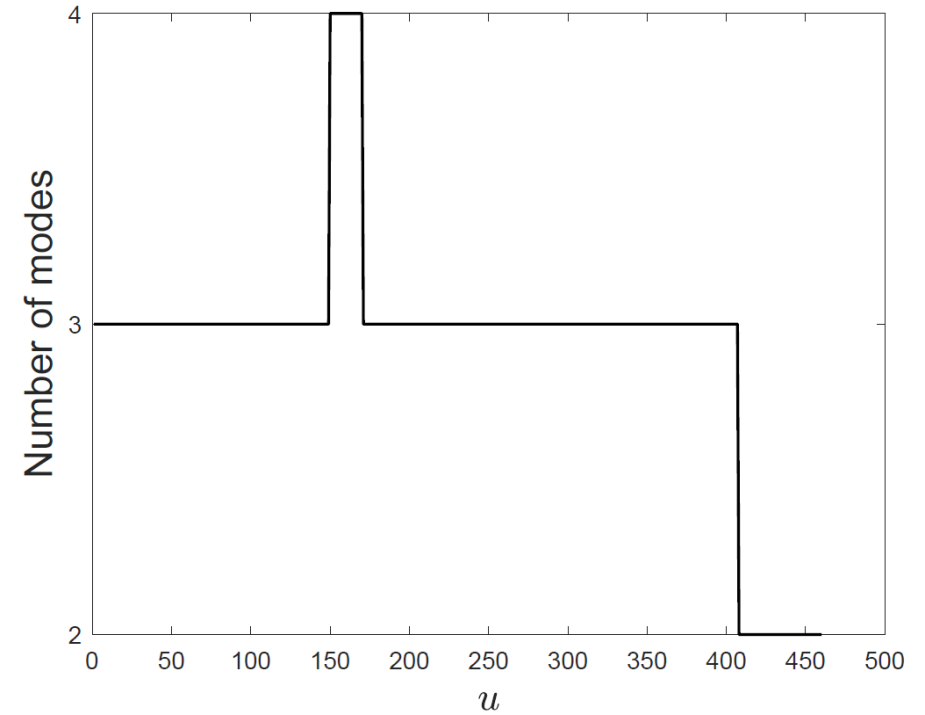
NOISY SPECTROGRAM



**BINARY MAP
ENCODED BY RLE**



RESULT



benefits: robustness to interference and noise